

Determination of the Location of Stomach Polyps from Endoscopic Examination Using Chan-Vese Segmentation Which is an Image Processing Technique

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Abstract— Stomach polyps are sessile or stalked lesions originating from stomach epithelial or submucosa and protruding to lumen. Observation rate of stomach polyps during endoscopic procedures is 2-6%. It is known that these are asymptomatic and also cause bleeding anemia, abdominal pain, gastric outlet obstruction. The most common polyps in the stomach are reported as hyperplastic polyps and hamman-Richardson gland polyps. In this study, a system has been designed for the detection of stomach polyps using image processing techniques from the endoscopy images of Gastroenterology clinic patients in Selcuk University Faculty of Medicine Hospital.

Keywords—Stomach Polyp, Image Processing, Chan-Vese Segmentation, Gastric Polyp

I. Introduction

Stomach polyps are more common in adults and they are single or multiple benign tumors. Polyps localized in the distal part of the stomach give more symptoms. When the polyps in the stomach are diagnosed, the cancer should be ruled out.

Stomach polyps are histologically classified as hyperplastic, adenomatous or inflammatory. Polypoid lesions such as leiomyomas and carcinoid tumors have been discussed in other threads. Hyperplastic polyps which comprises 80% of the cases are caused by the overgrowth of normal epithelium.

Approximately 30% of adenomatous polyps contain adenocarcinoma focus. Also 20% of adenocarcinoma can be found somewhere else in the stomach of the patients which has benign adenomatous polyps.

The incidence of cancer in adenomatous polyps increases with the size growth of the polyp. Lesions with handle and diameter that are smaller than 2 cm are not usually malignant. Approximately 10% of benign adenomatous polyps change in the direction of malignancy during their development [1]. For these reasons early detection is important. Therefore, studies in medical image processing need safe and effective image segmentation. Segmentation process is of paramount importance for the extraction of results in image processing. In our study, Chan-Vese segmentation method has been used. Because Chan-Vese method is a powerful and flexible geometric active contour model that can detect objects whose boundaries are not necessarily marked with a gradient. Similar to other active contour models, it aims an energy function to be minimized. Unlike others, its stopping term has not a dependency on image gradient, however. For this reason, it can achieve the segmentation of tissue structures, some of which would be difficult to define object boundaries due to the complexity of the tissue structures. The aim of this study is to perform a classification process for the endoscopy images that we have with Chan-Vese segmentation.

II. Material and Methods

Depending on the applications of medical image processing, removal of a significant portion of the image is the most important diagnostic step. This process is called "segmentation" in literature. In other words, segmentation is a key step in image definition and segmentation. Portion of the image obtained as a result of image segmentation is called "relevant area" [2]. In literature, many different methods have been used for segmentation process. Multiple gray level thresholding and rules-based approaches have been used for nodule detection while Lo and colleagues have proposed a two-tier system [3-4].

Accordingly, possible examples of nodules has been placed in the first stage, while in the second stage, nodular ones and the not nodular ones were separated using cellular artificial neural network (CANN). Another study following the detection of nodules using ANN realized by Xu and colleagues includes a set of forward orientation ANN and decision rules. In our study, Matlab R2015a Image Processing and Computer Vision toolbox has been used [5]. In our study, Matlab R2015a Image Processing and Computer Vision toolbox is used.

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A. Regional Based Active Credit Method

Image segmentation is a basic image processing operation used to distinguish objects within the image. One method of image segmentation method which was proposed by Chen-Vesa is the use of active credit and level set[6]. In level set theory, the curve pulls its lines to the desired edge and boundaries during the evolution. On the other hand, in active credit method, the first ideas is to use a deformable model and to minimize the energy function for each iteration. For active credit, two methods are used which are edge based and region based. While an edge detector is used for edge based method, detection of background and foreground is used for region based method[7]. In many cases as smooth segmentation can be realized for edge based method due to the basence of a global limiting on the image. On the other hand, region based method is advantageous than edge based method, because the first placed curve is solid and insensitive to the noise. However, the disadvantage of region based method is that it leads to false image segmentation occasionally. The basic idea of this method is that the closed curve (credit) achieve results starting with the first mask (a square shape, etc.) and then through expansion or contraction based on image restrictions. This process is done by minimizing the energy function and is known as the evolution of credit. Active credit formulation is based on two-dimensional Lipschitz function defined in the image plane. his function is called level set function. Initial level set function is named a signal distance function (SDF)[8]. Level set function $\phi = (x, y)$ is a two-dimensional Lipschitz function and it is applied for showing the credit values. Also, closed credit C curve can be shown indirectly by the zero level in ϕ' .

Credit can be positive or negative or it can be between the two. The credit development can be expressed with the equation of $\frac{\partial c}{\partial t} = \frac{\partial \phi(x,y)}{\partial t}$. If $\phi(x,y)=0$, C1 express a point on the curve. If $\phi(x,y) > 0$, C3 express the outside of the curve and if $\phi(x,y) < 0$, C2 express the inside of the curve.

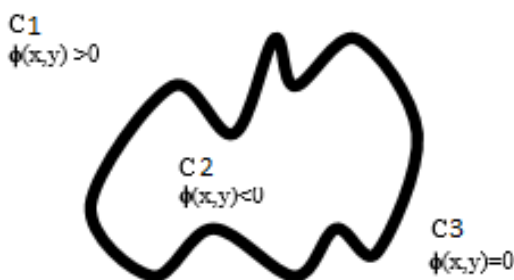


Fig. 1: Credit Development

Heaviside function is used to prevent sudden transitions from zero to 1 or 1 to zero on C curve. Therefore, the system output is guaranteed to be stable. Also, the outside area is expressed by $(1 - H(\phi))$.

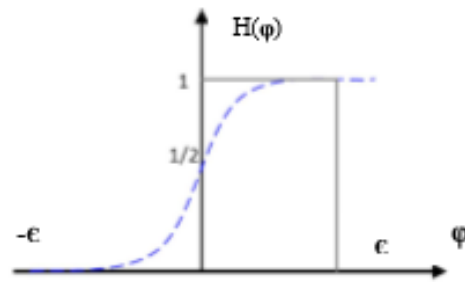


Fig. 2: Heaviside Function

$$H(\phi) = \begin{cases} 1 & \phi > \epsilon \\ \frac{1}{2} \left(1 + \frac{\phi}{\epsilon} + \frac{1}{\pi} \sin\left(\frac{\pi\phi}{\epsilon}\right) \right) & |\phi| < \epsilon \\ 0 & \phi < -\epsilon \end{cases} \quad (2)$$

The energy function can be shown as equation 3.

$$F = \mu \cdot \text{uzunluk}(C) + v \cdot \text{Alan}(ici(C)) + \lambda_1 \int_{ici(C)} |I(x,y) - u|^2 dx dy + \lambda_2 \int_{dışı(C)} |I(x,y) - v|^2 dx dy \quad (3)$$

In equation 3, I express the image and u and v are constants related to C. Also, μ , λ_1 and λ_2 are positive constants. For numerical calculations, λ_1 and λ_2 are set to 1 and v is set to 0. Taking into account the minimization problem, to minimize the energy function according to v and y, ϕ is fixed. Thus, u and v related to ϕ can be shown as following.

$$u = \frac{\int_{\Omega} I(x,y) H(\phi(x,y)) dx dy}{\int_{\Omega} H(\phi(x,y)) dx dy}$$

$$v = \frac{\int_{\Omega} I(x,y) (1 - H(\phi(x,y))) dx dy}{\int_{\Omega} (1 - H(\phi(x,y))) dx dy} \quad (4)$$

Here, u and v can be indicated as inside and outside areas. To update the curve, the level set function has to be restarted. The restarted function can be shown as in equation 5.

$$\phi^{t+1} = \phi^t - \Delta t \cdot S(\phi_0) \cdot G(\phi) \quad (5)$$

Zero level set limits the calculation with a narrow band around. The structure in Fig. 3 is named as narrow band. When zero level set approaches to the edge of the narrow band, the level set function is restarted. The narrow band is recalculated. Restart is not required while ϕ is calculated for the whole image. Because restart does not cause an effective

impact on the result while ϕ is calculated. Therefore, restart can be negligible. [9]



Fig. 3: Narrow Band innermost curve represents the zero level set.

III. Result and Discussion

Endoscopy images belonging to the patient are shown in Fig. 1(a), Fig. 2(a) and Fig. 3(a). The applications of Chan-Vese segmentation are shown in Fig. 1(b) Fig. 2(b) and Fig. 3(b) and Masked images of Chan-Vese segmentation process results are shown in Fig. 1(c), Fig. 2(c) and Fig. 3(c).

Original Image

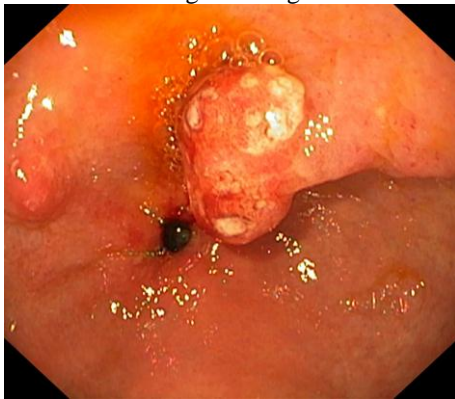


Fig. 4(a)

Chan-Vese Segmentation

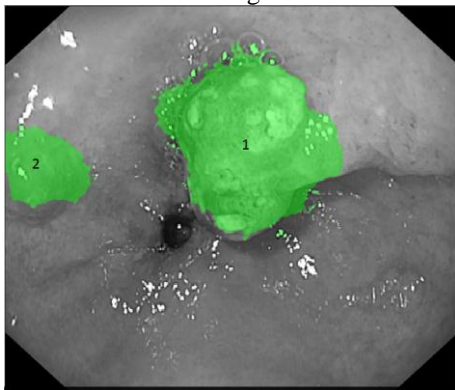


Fig. 4(b)

Masked Image

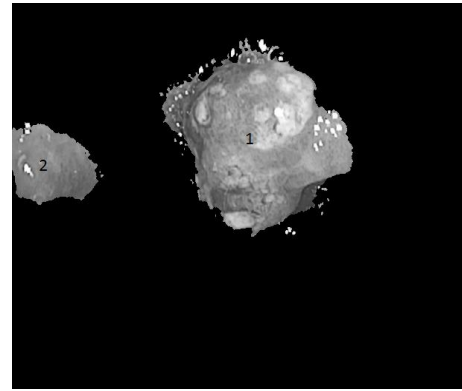


Fig. 4(c)

Original Image

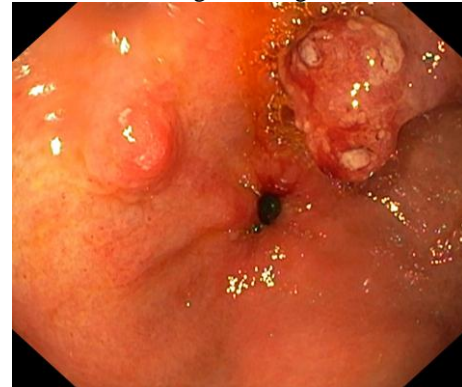


Fig.5(a)

Chan-Vese Segmentation

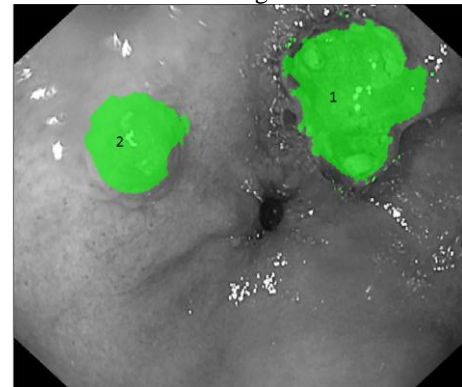


Fig. 5(b)

Masked Image

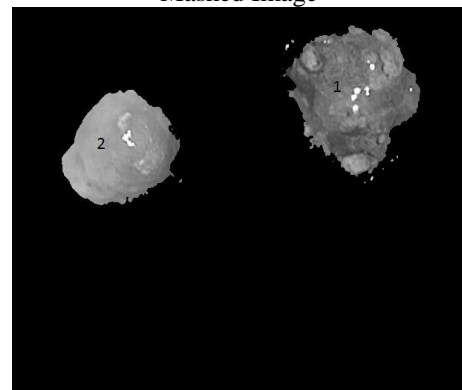


Fig. 5(c)

Original Image

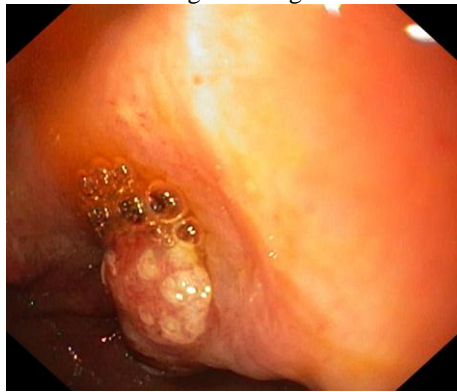


Fig. 6(a)

Chan-Vese Segmentation

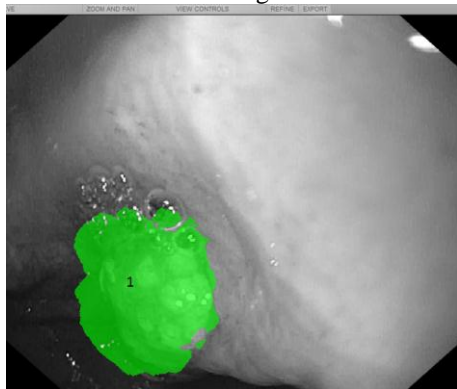


Fig. 6(b)

Masked Image

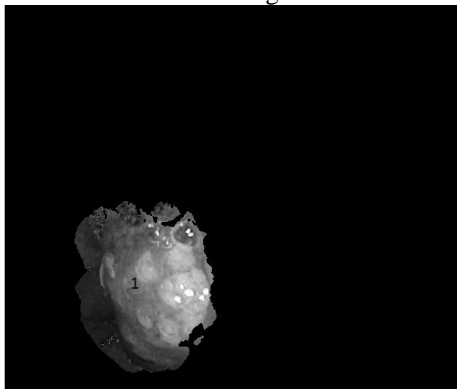


Fig. 6(c)

According to the masking method applied based on Chan-Vese segmentation method in image processing, during the evaluation of the performance of detecting polyps, success performance of the indicated polyp area by the doctor and the polyp are resulting from our study is shown in Table 1.

TABLE I. POLYP ARE RESULTING

Total Pixel Count / The number of pixels produced					
	Image 1(1)	Image 1(2)	Image 2(1)	Image 2(2)	Image 3(1)
Expert	28690	14414	47485	9216	42000
Study	32542	16328	50592	11863	26988

As a result of the comparison between the polyps determined by the doctor and resulted from our study, it seems that we achieved a successful outcome of %88 from Fig. 4(1), % 88 for Fig 4(2), %93,8 for Fig 5(1), %77,6 for Fig 5(2) and %64,2 for Fig 6(1).

IV. Conclusion

In this study, it is seen that Chan-Vese segmentation method can be used for the determination of stomach polyps and successful results can be obtained. For other studies, different segmentation processes are expected to produce better results. Studies will continue along with this thought.

Acknowledgements

. Appreciations to the doctors and the staff of Selcuk University, Faculty of Medicine Hospital, Gastroenterology clinic for their support in obtaining pictures necessary for our study. This study has been supported by Selcuk University's Scientific Research Unit (BAP)

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